



Consommation
et Corporations Canada

Consumer and
Corporate Affairs Canada

Bureau des brevets

Patent Office

Ottawa Canada
K1A 0G9

(11) (C) 1,297,368

(21) 536,577

(22) 1987/05/07

(45) 1992/03/17

(52) 128-104

(51) INTL.CL.³ A61K-9/58

(19) (CA) CANADIAN PATENT (12)

(54) Pulsed Drug Delivery

(72) Ayer, Atul D. , U.S.A.
Theeuwes, Felix , U.S.A.
Wong, Patrick S.L. , U.S.A.

(73) Alza Corporation , U.S.A.

(30) (US) U.S.A. 06/861,188 1986/05/09

(57) 21 Claims

Canada

004 1114 1114 11

1
2 PULSED DRUG DELIVERY
3

4 This invention pertains to a novel dosage form useful for
5 the pulsed delivery of a beneficial drug. The dosage form, after an
6 interval of time, can deliver a single pulse or dose of drug, or the
7 dosage form can deliver an initial pulse or dose of drug followed by a
8 delayed pulse or dose of drug.
9

10 BACKGROUND OF THE INVENTION
11

12 Many beneficial drugs are administered at a definite time
13 for their beneficial effects. For example, sleeping aids that help in
14 falling asleep are usually taken before bed and then, if needed, at a
15 later time, say four or five hours later. Then too, the symptomatic
16 relief of anxiety and tension, and the relief from pain and inflamma-
17 tion, usually requires an initial pulse or first dose supplemented at a
18 later interval by another pulse or second dose. The pulsatile delivery
19 of drugs having a short half-life, that is drugs that lose one-half of
20 their therapeutic activity because the drug is metabolized or excreted,
21 require pulsed administration at recurring intervals. Also, it is
22 often desirable to administer a drug in a form that makes the drug
23 available at a later time for a pulsed delivery of the drug. The need
24 for pulsed delivery arises during a circadian or chronological
25 cycle, for drugs with a pronounced first post effect and for drugs
26 which on continuous low level may lead to tolerance.

27 Prior to this invention, drugs with short half-lives were
28 often administered to a recipient once-or-twice in separate dosage



1 forms during a given time span, for example one-or-two doses to obtain
2 the benefit of the drugs pharmacokinetic activity. This type of
3 repeated dosing is accompanied with shortcomings. For example, when a
4 drug is administered at bed time the presently available prior art
5 dosage forms requires repeated dosing the recipient and interrupting
6 the sleep for the next dose. Then too, a recipient on a therapeutic
7 program often forgets to take the next dose, and this lack of compli-
8 ance leads to a drug-free interval during which interval the recipient
9 does not get the benefit of the next needed dose.

10 It is immediately apparent in the light of the above pre-
11 sentation that a pressing need exists for a dosage form that can delay
12 the delivery of a drug and then deliver a pulsed dose of drug. It is
13 apparent also that a pressing need exists for a dosage form that can
14 immediately deliver a pulsed dose of drug followed by a drug-free
15 interval and then deliver a pulsed dose of drug. It will be appre-
16 ciated by those versed in the dispensing art, that if a novel and
17 unique dosage form is made available for executing a therapeutic
18 program comprising pulsed and delayed drug delivery patterns, such a
19 dosage form would have a practical application and it would also
20 represent a valuable contribution to the medical and veterinary arts.

21 OBJECTS OF THE INVENTION

22 Accordingly, in view of the above presentation, it is an
23 immediate aspect of this invention to provide a novel and useful
24 dosage form that represents an unexpected improvement in the dispen-
25 sing art and substantially overcomes the disadvantages known to the
26 prior art.

27 Another aspect of the present invention is to provide a
28 dosage form that can deliver a pulsed dose of a beneficial drug.

1 Another aspect of the present invention is to provide a
2 dosage form that can delay the delivery of the drug from the dosage
3 form, and then deliver a pulsed dose of the drug.

4 Another aspect of the present invention is to provide a
5 novel dosage form comprising means for delivering an initial pulsed
6 dose of drug, means for maintaining a drug-free interval, and means
7 for delivering a later pulsed dose of drug at a later time.

8 Another aspect of the present invention is to provide a
9 novel dosage form that overcomes the limited functionality of conven-
10 tional dosage tablets, and which novel dosage form can preform a drug
11 program comprising delivering a drug at a pulsed rate and for a pulsed
12 duration as needed to achieve a desired therapeutic program.

13 Another aspect of the invention is to provide a dosage form
14 comprising two doses of drug in a single dosage form that can be used
15 for twice a day dosing of the drug.

16 Another aspect of the present invention is to provide a
17 novel dosage form manufactured in the form of a drug delivery device
18 comprising means for delivering a pulsed dose of drug, means for
19 providing a drug-free interval, and means for then providing a recur-
20 ring pulsed dose.

21 Another aspect of the invention is to provide a dosage form
22 comprising two doses in a single dosage form.

23 Another aspect of the present invention is to provide a
24 dosage form comprising an exterior member for providing an immediate
25 pulsed dose of drug, and an internal member for providing a delayed
26 pulsed dose of drug.

27 Other aspects, features and advantages of the invention will
28 be more apparent to those versed in the dispensing art from the following

specification, taken in conjunction with the drawing figures and the accompanying claims.

Summary of the Invention

Accordingly, the invention herein comprises a dosage form for the delivery of a beneficial drug formulation to an environment of use, comprising:

(a) a wall comprising in at least a part a semipermeable composition permeable to the passage of an external fluid present in the environment of use and substantially impermeable to the passage of a beneficial drug formulation, which wall surrounds and defines:

(b) a compartment;

(c) a first layer comprising a beneficial drug formulation in the compartment;

(d) a second layer comprising a hydrogel composition that increases in volume in the presence of fluid that enters the compartment;

(e) means for delaying the delivery of drug formulation from the compartment, which means comprises a drug-free composition that surrounds the first and second layer; and,

(f) at least one exit means in the wall for communicating the exterior of the dosage form with the compartment for delivering the drug formulation from the dosage form.

The invention further comprises a dosage form for delivering a beneficial drug formulation to an environment of use, wherein the dosage form comprises:

(a) a wall comprising in at least a part a semipermeable

composition permeable to the passage of an external fluid present in the environment of use and substantially impermeable to the passage of a beneficial drug formulation, said wall surrounding:

(1) a first layer comprising a dosage amount of a beneficial drug formulation;

(2) a second layer comprising a hydrogel composition that expands in the presence of fluid;

(3) means coated around the first and second layers for delaying the release of the drug formulation from the dosage form;

10 (b) at least one exit means in the wall for releasing the beneficial dosage formulation from the dosage form; and,

(c) a dosage amount of a beneficial drug formulation in contact with the exterior surface of the wall of the dosage form.

BRIEF DESCRIPTION OF THE DRAWING FIGURES

In the drawing figures, which are not drawn to scale, but are set forth to illustrate various embodiments of the invention, the drawing figures are as follows:

20 Figure 1 is a general view of a dosage form provided by the invention, which dosage form is designed and shaped for oral administration, for delayed, or pulsed patterns of drug delivery to the gastrointestinal tract;

Figure 2 is a view of an osmotic dosage form provided by the invention comprising an exterior dosage amount of drug for the initial pulsed delivery of the drug to the gastrointestinal tract;

Figure 3 is an opened view of a dosage form provided by the invention, which dosage form delays the pulsed delivery of a dose amount of drug to the gastrointestinal tract;

1297369

67696-104

Figure 4 is an opened view of a dosage form provided by the invention which dosage form provides an initial pulsed dose of drug followed by a drug-free interval and then another pulsed dose of drug; and,

Figure 5 is an opened view of another embodiment of the invention for providing a first dose of drug and at a later time a second dose of drug.

In the drawing figures and in the specification, like parts in related figures are identified by like numbers. The
10 terms appearing earlier in the specification and in the description of the drawing figures, as well as embodiments thereof, are further described elsewhere

1 in the disclosure.

2 DETAILED DESCRIPTION OF THE
3 DRAWING FIGURES

4 Turning now to the drawing figures in detail, which drawing
5 figures are an example of the dosage form provided by the invention,
6 and which examples are not to be construed as limiting, one example of
7 the dosage form is illustrated in Figure 1 and designated by the
8 numeral 20. In Figure 1, dosage form 20 comprises a body member 21
9 comprising a wall 22 that surrounds and forms an internal compartment
10 not seen in Figure 1. Dosage form 20 further comprises at least one
11 exit means 23 for connecting the interior of dosage form 20 with the
12 exterior environment of use.

13 Figure 2 illustrates dosage form 20 of Figure 1 comprising
14 body 21, wall 22, exit means 23 and exterior lamina 24. Exterior
15 lamina 24 comprises a dosage unit amount of drug for an initial pulsed
16 dose of drug to the environment of use, the gastrointestinal tract of
17 a warm-blooded animal. The initial pulse is the first dose of drug.
18 Exterior lamina 24 comprises from about 0.1 to 99.9 weight percent
19 (wt. %) of a drug, and from 99.9 to 0.1 wt. % of a pharmaceutically
20 acceptable carrier for the drug, with the total wt. % of all lamina
21 24 forming members equal to 100%. In a more preferred embodiment
22 the initial pulse dose is from 10 to 80 wt % and from 90 to 20 wt %
23 carrier. The carrier is a means for coating the drug onto the exterior
24 surface of the wall, and the carrier comprising lamina 24 onto the
25 exterior surface of wall 22. In the fluid environment of use, the
26 carrier releases the drug thereby providing the initial or first
27 pulsed dose of the drug to the environment of use. The carrier re-
28 leases the initial pulsed dose in from greater than zero time up to 1

1 hour, and in a presently preferred pulsed dose time of from several
2 minutes up to 30 minutes. Typical carrier means include a hydrophilic
3 polymer, that are in a presently preferred embodiment a member selected
4 from the group consisting of hydroxymethyl cellulose, hydroxyethyl
5 cellulosa, hydroxypropyl cellulose, hydroxypropyl methylcellulose and
6 hydroxypropyl ethylcellulose.

7 Figure 3 is a view of dosage form 20 seen in opened view
8 with wall 22 sectioned at 25 for illustrating the internal structure
9 of dosage form 20. In Figure 3, osmotic dosage form 20 comprises body
10 21, wall 22 that surrounds and defines an interior compartment 26 and
11 at least one exit means 23. Wall 22 of dosage form 20 comprises at
12 least in part, or totally, a composition that is permeable to the
13 passage of an exterior fluid present in the environment of use, and it
14 is substantially impermeable to the passage of drug and other ingre-
15 dients present in compartment 26. Wall 22 is comprised of a polymeric
16 composition that is inert and maintains its physical and chemical
17 integrity during the life time of dosage form 20. The phrase,
18 "physical and chemical integrity" denotes wall 22 does not lose its
19 structure and it does not change during the dispensing life of dosage
20 form 20. Typical materials for forming wall 22 comprise selectively
21 semipermeable polymers known to the art as osmosis and reverse osmosis
22 polymers. These polymeric compositions comprise a cellulose ester,
23 cellulose ether, cellulose ester-ether, cellulose acylate, cellulose
24 diacylate, cellulose triacylate, cellulose acetate, cellulose diacetate,
25 and cellulose triacetate. In a presently preferred embodiment wall 22
26 is a composition comprising cellulose acetate having an acetyl content
27 of 32%, cellulose acetate having an acetyl content of 39.3%, hydroxy-
28 propyl methylcellulose and polyethylene glycol. In one example wall

1 22 is a composition comprising from 15 to 45 wt. % cellulose acetate
2 having an acetyl content of 32%; 15 to 45 wt. % cellulose acetate
3 having an acetyl content of 39.8%; from 5 to 35 wt. % of hydroxypropyl
4 methylcellulose; and from 5 to 35 wt. % polyethylene glycol 3350.

5 Internal compartment 26 in one preferred embodiment houses
6 a first layer comprising a beneficial drug formulation 27, identified
7 by dots, and a hydrogel carrier 28, identified by dashes, for drug
8 formulation 27. Hydrogel carrier means 28 comprises a hydrophilic
9 composition that is noncross-linked, or lightly cross-linked, and it
10 possesses the ability to form a dispensable, pulsed drug formulation
11 by homogeneously blending with drug formulation 27. In operation,
12 hydrogel carrier means 28 absorbs and/or imbibes fluid and expands to
13 form a dispensable pulsed formulation that is released from dosage
14 form 20 transporting drug formulation 27 therewith. The pulsed dose
15 has generally a pulsed duration of 10 minutes to 200 minutes, and more
16 preferably 20 minutes to 40 minutes. Generally, the dosage unit
17 amount of drug blended with the hydrogel carrier means is about 1 to
18 80 wt. %.

19 Internal compartment 25 houses a second layer 29 comprising
20 a hydrogel member and in a presently preferred embodiment an osmagent
21 blended with the hydrogel member. The hydrogel comprising second
22 layer 29 exhibits fluid absorbing and/or fluid imbibing properties.
23 The hydrogel comprised of a hydrophilic polymer interacts with water
24 and aqueous biological fluids and swells or expands to an equilibrium
25 state. The hydrogel exhibits the ability to swell in aqueous fluid
26 and retain a significant portion of the absorbed or imbibed fluid
27 within the polymer structure. In operation, the first layer and the
28 second layer cooperate to deliver the drug formulation from dosage

1 form 20. In operation, the second layer 29 absorbs fluid, expands and
2 exerts pressure against the first layer. Simultaneously, the first
3 layer absorbs fluid and forms a dispensable formulation. By the
4 combined operation of the first and second layers, with the second
5 layer expanding against the first layer and urging it from the compart-
6 ment, and with the first layer forming a dispensable formulation, the
7 drug formulation is delivered from the dosage form.

8 The hydrogel comprising carrier means 28 and
9 second layer 29 swell or expand to a very high degree, usually exhibit-
10 ing from their nonhydrated state a 2 to 50 fold increase in volume.
11 The hydrogel comprising carrier means 28, for the purpose of this
12 invention, is a different hydrogel than the hydrogel comprising second
13 layer 29. The hydrogel comprising carrier means 28 and the hydrogel
14 comprising second layer 29, in operation, cooperate to deliver the
15 pulsed dose of drug from the dosage form. Representative hydrophilic
16 hydrogels consists of a member selected from the group consisting of
17 poly(hydroxyalkyl methacrylate) having a molecular weight of 20,000 to
18 5,000,000; poly(vinylpyrrolidone) having a molecular weight of about
19 10,000 to 360,000; poly(vinyl alcohol) having a low acetate content
20 and lightly cross-linked with glyoxal, formaldehyde, glutaraldehyde
21 and having a degree of polymerization from 200 to 30,000;
22 poly(ethylene oxide) having a molecular weight from 10,000 to
23 5,000,000; acidic carboxy polymers known as carboxypolymethylene and
24 carboxyvinyl polymers, a polymer consisting of acrylic acid lightly
25 cross-linked with polyallyl-sucrose and sold under the trademark Carbopol®,
26 acidic carboxy polymer having a molecular weight of 200,000 to
27 6,000,000, including sodium acidic carboxyvinyl hydrogel and potassium
28 acidic carboxyvinyl hydrogel; Cyanamer® polyacrylamide; and the

1 like. The representative polymers are known to the art in Handbook of
2 Common Polymers, by Scott and Roff, published by the Chemical Company,
3 Cleveland, OH; ACS Symposium Series, No. 31, by Ratner and Hoffman,
4 pp. 1 to 36, 1976, published by the American Chemical Society; and in
5 Recent Advances In Drug Delivery Systems, by Schacht, pp. 259 to 278,
6 published by Plenum Press, N.Y.

7 Second layer 29 can comprise optionally an osmagent blended
8 with the hydrophilic polymer. The osmagent is present to aid in
9 imbibing exterior fluid through wall 22 and into second layer 29. The
10 dual action of the osmagent imbibing fluid and the hydrogel imbibing
11 fluid results in an increase in the expansion of layer 29 thereby
12 assuring substantially complete delivery of drug formulation 27 from
13 dosage form 20. Osmagents are known also as osmotically effective
14 solutes and osmotically effective compounds. The osmagents are soluble
15 in fluid that enters the dosage form, and they exhibit an osmotic
16 pressure gradient across semipermeable wall 22 against an exterior
17 fluid. Osmotically effective osmagents useful for the present purpose
18 include magnesium sulfate, magnesium chloride, sodium chloride, lithium
19 chloride, potassium sulfate, sodium sulfate, sodium carbonate, lithium
20 sulfate, sodium sulfate, and the like. The osmagent is usually present
21 as a particle, powder, granule, or the like. The amount of active
22 osmagent homogeneously or heterogeneously blended with the hydrophilic
23 hydrogel in the second layer is usually from 0.01% to 45%, or higher.
24 The osmotic pressure in atmospheres, ATM, of the osmagent suitable for
25 the invention will be greater than zero ATM, generally from zero ATM
26 up to 500 ATM, or higher. The osmotic pressure of an osmagent is
27 measured in a commercially available osmometer that measures the vapor
28 pressure difference between pure water and the solution to be analyzed,

1 and according to standard thermodynamic principles the vapor pressure
2 ratio is converted into an osmotic pressure difference. The osmometer
3 used for the present measurements is identified as Model 1001-A Vapor
4 Pressure Osmometer, manufactured by Knauer and distributed by Utopia
5 Instrument Co., Joliet, Illinois.

6 Dosage form 20 of Figure 3 comprises internal delayed coat
7 30 that surrounds the first layer and the second layer. Delayed coat
8 30 is a drug-free coat. Delayed coat 30 provides an interval of time
9 during which dosage form 20 postpones the delivery of drug formulation
10 27. Delayed coat 30 in its initial dry state is about 0.1 mm to 10 mm
11 thick, and in a more presently preferred range delayed coat 30 is
12 about 4 to 7 mm thick. Delayed coat 30 is a means for delaying the
13 delivery of drug formulation for about 1 hour to 12 hours, preferably
14 2 hours to 9 hours, and in a presently more preferred embodiment it
15 provides a drug-free interval of 3 hours to 6 hours. Delayed coat 30
16 comprises initially a dry hydrophilic polymer such as a member selected
17 from the group consisting of hydroxypropyl methylcellulose, hydroxy-
18 propylcellulose, methylcellulose, carboxymethylcellulose,
19 hydroxyethylcellulose, hydroxymethylcellulose, and the like. Delayed
20 coat 30 can comprise also a member selected from the group consisting
21 of poly(oxyethylene), poly(vinyl pyrrolidone), carboxyvinyl polymer,
22 and the like.

23 Figure 4 illustrates another dosage form 20 provided by the
24 invention. Dosage form 20 makes available the pulsed delivery of drug
25 followed by a drug-free interval, and then a final pulsed dose of
26 drug. This dosage form also exemplifies a single dosage form comprising
27 two distinct and independent doses of drug. Dosage form 20 of Figure
28 4 comprises exterior pulsed drug coat 24 that surrounds in at least a

1 part exterior wall 22 of body 21 of dosage form 20. Dosage form 20
2 also comprises an exit passageway 23 that communicates the exterior of
3 dosage form 20 with internal compartment 26. Internal compartment 26
4 comprises a first layer that comprises drug formulation 27 and carrier
5 means 28, and a second layer comprising a hydrogel composition 29. An
6 inner positioned delayed, drug-free coat 30 is located between the
7 inside surface of wall 20 and it surrounds both inner contacting
8 layers in compartment 26. Dosage form 20, is sized, shaped and
9 designed for oral admittance into the gastrointestinal tract of a
10 warm-blooded animal including a human. Dosage form 20 is manufactured
11 as an osmotic device and it provides a pulsed-delayed-pulsed drug
12 pattern or first dose delay second dose in the manner described for
13 the above drawing figures.

14 Figure 5 illustrates another dosage form 20 provided by the
15 invention. Dosage form 20 of Figure 5 comprises body 21, wall 22
16 comprising at least in part a semipermeable composition, which wall is
17 sectioned at 25, exit means 23, exterior lamina 24 comprising a first
18 dosage amount of drug, interior drug release delaying lamina 30,
19 internal compartment 26 housing a second dosage amount of orally
20 administrable drug 27 and, optionally, a hydrogel 28.

21 The expression "exit means" as used herein comprises means
22 and methods suitable for releasing the pulsed dose from compartment
23 26. The expression includes at least one passageway or orifice that
24 passes through wall 22 for communicating with compartment 26. The
25 expression "at least one passageway" includes aperture, orifice, bore,
26 pore, porous element through which drug can migrate, a hollow fiber,
27 capillary tube and the like. The expression includes also a material
28 that erodes or is leached from wall 22 in the fluid environment of use

1 to produce at least one passageway in the dosage form. Representative
2 materials suitable for forming at least one passageway, or a multipli-
3 city of passageways include an erodible poly(glycolic) or poly(lactic)
4 acid member in the wall, a gelatinous filament, leachable materials
5 such as fluid removable pore forming polysaccharides, salts or oxides,
6 and the like. A passageway or a plurality of passageways can be
7 formed by leaching a material such as sorbitol from the wall to produce
8 a controlled release passageway. The passageway can have any shape,
9 such as round, triangular, elliptical, and the like. The device can
10 be constructed with one or more passageways in spaced apart relation
11 on more than a single surface of a dosage form. Passageways and
12 equipment for forming passageways are disclosed in U. S. Pat. Nos.
13 3,916,899; 4,063,064 and 4,028,864. Passageways of controlled dimen-
14 sions formed by leaching are disclosed in U. S. Pat. No. 4,200,092.

15 The expression "drug formulation", as used herein, denotes
16 any beneficial agent, compound, or composition of matter, that can be
17 delivered by the dosage form in pulsed doses : first and second doses
18 to produce a beneficial, therapeutic results. Drugs for the
19 present purpose include any physiologically or pharmacologically
20 active substance that produces a local or a systemic effect in animals.
21 The term animals includes warm-blooded mammals, humans, primates,
22 household, sport, farm and zoo animals. The term "physiologically" as
23 used herein denotes the administration of a drug to produce normal
24 levels and functions. The term "pharmacologically" denotes variations
25 in responses to various amounts of drug administered to the host.
26 Stedman's Medical Dictionary, 1966, published by Williams and Wilkins,
27 Baltimore, MD. The active drugs that can be delivered include inorganic
28 and organic drugs without limitations, drugs that can act on the

1 central nervous system, depressants, hypnotics, sedatives, psychic
2 energizers, tranquilizers, anticonvulsants, muscle relaxants, anti-
3 parkinson agents, anti-inflammatories, local anesthetics, muscle
4 contractants, antimicrobials, antimalarials, hormonal agents, contra-
5 ceptives, diuretics, sympathomimetics, antiparasitics, neoplastics,
6 hypoglycemics, ophthalmics, electrolytes, diagnostics, cardiovascular
7 drugs, and the like. The beneficial drugs are known to the art in
8 Pharmaceutical Sciences, by Remington, 14 Ed., 1979 published by Mack
9 Publishing Co., Easton, PA.; The Drug, The Nurse, The Patient,
10 Including Current Drug Handbook, 1974-76 by Falconer et al., published
11 by Sounder Company, Philadelphia, PA.; and Physician's Desk Reference,
12 40th Ed., 1986, published by Medical Economics Co., Oradell, N.J.

13 The wall of the dosage form, and the exterior pulsed re-
14 lease lamina can be formed in one technique using the air suspension
15 procedure. This procedure consists in suspending and tumbling de-
16 layed, coated bilayers in a current of air and a wall forming, or
17 outer pulsed lamina composition, until in either operation the wall or
18 the pulsed lamina is applied to the delayed coated bilayers. The air
19 suspension procedure is well-suited for independently forming the wall
20 of the pulsed lamina. The air suspension procedure is described in
21 U. S. Pat. No. 2,799,241; in J. Am. Pharm. Assoc., Vol. 48, pp. 451
22 to 459, 1959; and, *ibid*, Vol. 49, pp. 82 to 84, 1960. The osmotic
23 dosage-pulsed-delayed systems can also be coated with the wall forming
24 composition, or the lamina pulsed composition with a Wurster® air
25 suspension coater, using for example methylene dichloride - methanol
26 cosolvent. The Aermatic® air suspension coater can be used also
27 employing a cosolvent. Other wall and laminating techniques such as
28 pan coating can be used for providing the dosage form. In the pan

1 coating system the wall forming, or the pulsed lamina forming, compo-
2 sitions are deposited by successive spraying of the composition on the
3 delayed coated bilayers accompanied by tumbling in a rotating pan. A
4 pan coater is used to produce a thicker wall or lamina. A larger
5 volume of methanol can be used in a cosolvent to produce a thinner
6 wall or lamina. Finally, the wall or lamina coated compartments are
7 dried in a forced an oven at 50°C for a week, or in a temperature and
8 humidity controlled over for 24 hours at 50°C and 50 relative humidity,
9 to free the dosage form of solvent. Generally, the wall formed by
10 these techniques have a thickness of 2 to 20 mils with a presently
11 preferred thickness of 4 to 10 mils. The exterior pulsed dose lamina
12 generally will have a thickness of 0.5 to 15 mils, usually 0.5 to
13 7.5 mils.

14 Exemplary solvents suitable for manufacturing the wall or
15 the lamina include inert inorganic and organic solvents that do not
16 adversely harm the wall, the lamina and the final dosage system. The
17 solvents broadly include a member selected from the group consisting
18 of an alcohol, ketone, ester, ether, aliphatic hydrocarbon, halogenated
19 solvents, cycloaliphatic solvents, aromatic, heterocyclic, aqueous
20 solvents, and mixtures thereof.

21 The dosage form of the invention is manufactured by standard
22 techniques. For example, in one manufacture the beneficial drug and
23 other ingredients comprising the first layer facing the exit means are
24 blended and pressed into a solid layer. The layer possesses dimen-
25 sions that correspond to the internal dimensions of the area the layer
26 is to occupy in the dosage form and it also possesses dimensions
27 corresponding to the second layer for forming a contacting arrangement
28 therewith. The drug and other ingredients can be blended also with a

1 solvent and mixed into a solid or semisolid form by conventional
2 methods such as ballmilling, calendering, stirring or rollmilling and
3 then pressed into a preselected shape. Next, a layer of hydrogel is
4 placed in contact with the layer of drug in a like manner. The
5 layering of the drug formulation and the hydrogel layer can be fabri-
6 cated by conventional two-layer press techniques. The two contacted
7 layers are first coated with a delayed drug-free overcoat and then
8 with the outer wall. The drug-free delayed composition can be applied
9 by press coating, molding, spraying, dipping, and air suspension
10 procedures. The air suspension and air tumbling procedure comprises
11 in suspending and tumbling the pressed, contacting first and second
12 layers in a current of air containing the delayed-forming composition
13 until the first and second layers are surrounded by the delayed
14 composition.

15 In another manufacture, the dosage form is manufactured by
16 the wet granulation technique. In the wet granulation technique the
17 drug and the ingredients comprising the first layer are blended using
18 an organic cosolvent, such as isopropyl alcohol-methylene dichloride
19 80/20 v/v (volume/volume) as the granulation fluid. The ingredients
20 forming the first layer are individually passed through a 40 mesh
21 screen and then thoroughly blended in a mixer. Next, other ingre-
22 dients comprising the first layer are dissolved in a portion of the
23 granulation fluid, the cosolvent described above. Then, the latter
24 prepared wet blend is slowly added to the drug blend with continual
25 mixing in the blender. The granulating fluid is added until a wet
26 blend is produced, which wet mass blend is then forced through a 20
27 mesh screen onto oven trays. The blend is dried for 18 to 24 hours at
28 35°C in a forced air oven. The dried granules are then sized with a

1 20 mesh screen. Next, magnesium stearate is added to the dry screened
2 granule blend, and this blend passed through an 80 mesh screen. The
3 granulation is then put into milling jars and mixed on a jar mill for
4 5 to 10 minutes. The composition is pressed into a layer, for example
5 in a 3-station Manesty® layer press. The speed of the press is set at
6 30 rpm and the maximum load set at 2 tons. The first layer is pressed
7 against the composition forming the second layer and the bilayer
8 tablets are fed to the Killiam® dry Coata press and surrounded with the
9 drug-free coat followed by the exterior wall solvent coating.

10 Another manufacturing process that can be used for
11 providing the compartment-forming composition comprises blending the
12 powdered ingredients in a fluid bed granulator. After the powdered
13 ingredients are dry blended in the granulator, a granulating fluid,
14 for example poly(vinylpyrrolidone) in water, is sprayed onto the
15 powders. The coated powders are then dried in the granulator. This
16 process granulates all the ingredients present therein while adding
17 the granulating fluid. After the granules are dried, a lubricant such
18 as stearic acid or magnesium stearate is added to the granulator. The
19 granules are then pressed in the manner described above.

20 DESCRIPTION OF EXAMPLES OF THE INVENTION

21 The following examples are merely illustrative of the
22 present invention and they should not be considered as limiting the
23 scope of the invention in any way, as these examples and other equiva-
24 lents thereof will become more apparent to those versed in the art in
25 the light of the present disclosure, the drawing figures and the
26 accompanying claims.

27 EXAMPLE 1

28 A dispensing device is manufactured for delivery a bene-

1297368

ARC 1335

1 ficial drug as follows: a first layer and a second layer are compressed
2 in contacting arrangement in a three layer press under a 1 1/2 ton
3 pressure head. The first layer is made from granules of a homogeneous
4 master blend comprising 570 g of polyethylene oxide having a molecular
5 weight of 200,000; 400 g of midazolam; and 30 g of hydroxypropylmethyl
6 cellulose. The ingredients are dry blended, then wetted with 350 ml
7 of anhydrous ethanol, followed by drying in an oven for 17 to 20 hrs
8 at 30°C. The dry granules then are passed through a 30 mesh screen.
9 The second layer is formed from a composition comprising 650 g of
10 polyethylene oxide having a molecular weight of 5,000,000; 230 g of
11 sodium chloride; 50 g of hydroxypropylmethyl cellulose; and 10 g of
12 ferric oxide. The materials comprising the second layer are blended
13 and then wetted with 950 ml of anhydrous ethanol. The wet granules
14 are dried at 30°C for 15 to 20 hrs in a forced air oven, and then
15 passed through a 20 mesh sieve.

16 The granules for the first layer forming composition are
17 transferred to the number 1 hopper, and the granules for the second
18 layer forming composition are added to the number 2 hopper of the
19 press. The first and second layers are pressed together with the
20 first layer weighing 12.5 mg and the second layer weighing 50.0 mg,
21 with a diameter of 4.76 mm.

22 A delay layer coating is applied with a Kilian® dry Coata
23 press. The pressed together layers are transferred to the Coata press
24 hopper, and a delay composition comprising hydroxypropyl cellulose is
25 dry coated around the first and second layers. The delay coated first
26 and second layers have a diameter of 7 mm.

27 Next, the delayed coated layers are transferred to an
28 Aeromatic® air suspension coater. The systems are surrounded with a

1 semipermeable wall-forming composition for applying a 4 mg wall per
2 system. The wall forming composition comprises 30 wt. % cellulose
3 acetate having an acetyl content of 39.8%; 30 wt. % cellulose acetate
4 having an acetyl content of 32%; 20 wt. % polyethylene glycol 400; and
5 20 wt. % hydroxypropylmethyl cellulose. The wall forming ingredients
6 are dissolved in a cosolvent comprising methylene chloride: methanol
7 (85:15 wt. %) to obtain 5% solids.

8 Finally, a first and a second passageway are drilled
9 through the wall for connecting the exterior of the dosage form with
10 the interior of the dosage form. A passageway is drilled on two
11 distant surfaces of the dosage form. The dosage forms are dried in a
12 forced air oven at 50°C for 40 hrs to remove all residual solvent.
13 The dosage forms are sized and shaped for oral admittance into the
14 gastrointestinal tract of a human.

15 EXAMPLE 2

16 The procedure of Example 1 is repeated in this example with
17 all manufacturing steps as previously set forth, except that in this
18 example the wall comprising the semipermeable composition is coated
19 with a pulsed coat of drug. The pulsed coat is applied to the exterior
20 surface of the wall from a composition comprising 50 wt. % midazolam,
21 25 wt. % hydroxypropyl cellulose and 25 wt. % tartaric acid, dissolved
22 in distilled water to obtain 15 wt. % solids. The pulsed coat applied
23 to each dosage form contains 10 mg of midazolam.

24 Next, a pair of passageways were drilled through the outer-
25 most pulsed coat and the wall for connecting the exterior of the wall
26 for connecting the exterior of the dosage form with its compartment.
27 The dosage form is dried as described previously.

28 The dosage form prepared according to the example releases

1297368

ARC 1325

1 the 10 mg of midazolam in about 10 minutes. The first pulsed release
2 is followed by a 3 1/2 hour drug-free period. The second dose of
3 midazolam is delivered in about 1/2 hour for 80% of the drug with
4 substantially all of the drug delivered in about 1 to 1 1/2 hours.

5 EXAMPLE 3

6 The procedures of Examples 1 and 2 are repeated in this
7 example. In this example, the first layer weighed 18.75 mg, the
8 second layer weighed 70 mg, the internal delay layer weighed 110 mg,
9 the wall weighed 4.5 mg and the outermost coat contained 15 mg of
10 midazolam. The dosage form released 15 mg of midazolam in a first 15
11 minute pulsed period, and delivered 7.5 mg of midazolam after a 3.5
12 hour delay.

13 EXAMPLE 4

14 The procedure of Example 1 is followed for manufacturing a
15 dosage form comprising two 6.5 mil (0.17 mm) passageways on two opposite
16 surfaces of the dosage form. The dosage form delivered the internally
17 housed midazolam after a 3.5 hour delay with 80% delivered in about 1/2
18 hour.

19 EXAMPLE 5

20 The procedures of Examples 1 and 4 are followed that the
21 interior housed delayed composition comprises hydroxypropylmethyl
22 cellulose 47.5 wt %; hydroxypropyl cellulose 50 wt. % and polyvinyl
23 pyrrolidone 2.5 wt. %.

24 EXAMPLES 6 and 7

25 The above procedure is repeated with the manufacturing
26 conditions as set forth, with one example comprising an internal delay
27 layer weighing 80 mg that release the drug after 2.8 hours; and another
28 internal delay coat weighing 120 mg that permits the dosage form to

1 deliver the drug after a 4.6 hour delay period of time.

2 EXAMPLE 8

3 A dosage form for use as a nighttime sleep-aid comprising
4 an exterior pulsed dose of diphenhydramine hydrochloride, and an
5 internal pulsed dose of diphenhydramine is made as follows: a first
6 layer comprising 50 mg of diphenhydramine hydrochloride, polyethylene
7 oxide having a molecular weight of 120,000 and hydroxypropylmethyl
8 cellulose, is pressed in contacting position to a second layer comprising
9 polyethylene oxide having a molecular weight of 5,000,000 and
10 sodium chloride. The two layers are first surrounded with a delay
11 coat comprising hydroxypropyl cellulose, and then with a wall comprising
12 cellulose triacetate having an acetyl content of 43.5% and
13 cellulose acetate having an acetyl content of 32%. The wall is coated
14 on its outer surface with an instant pulsed dose coat comprising 25 mg
15 of diphenhydramine hydrochloride, hydroxypropyl cellulose and citric
16 acid. The dosage form is made with a pair of spaced-apart passageways.
17 The dosage form is administered one at bed time for the relief
18 of sleeplessness. The dosage form delivers the outer pulsed dose and
19 after a 3 to 3 1/2 hour drug-free period, delivers the internal dose.
20 The dosage form is blister packed for ease of administration.

21 EXAMPLE 9

22 The procedure of Example 8 is repeated with the condition
23 as described previously except that in this example the dosage form
24 internally contained in the first layer 15 mg of doxylamine succinate,
25 and 10 mg of doxylamine succinate in the exterior coat. The dosage
26 form is administered about 30 minutes before retiring as nighttime
27 sleep aid.

28

EXAMPLE 10

1
2 A dosage form for the relief of menstrual pain and more
3 particularly menstrual and premenstrual pain and discomfort is made in
4 accordance with the above described procedures. The dosage form
5 comprises an internal first layer comprising 200 mg of acetaminophen,
6 34 mg of pamabron (2-amino-2-methyl-1-propanol-3-bromo-theophyllinate),
7 and 17 mg of pyrilamine maleate, polyethylene oxide having a molecular
8 weight of 120,000 and hydroxypropylmethyl cellulose, a second layer
9 comprising Cyanamer® A-370 a hydrogel polyacrylamide of about 200,000
10 molecular weight, and sucrose; and an outermost exterior pulsed coat
11 comprising 100 mg of acetaminophen, 16 mg of pamabron and 8 mg of
12 pyrilamine maleate. The dosage form after administration delivers an
13 instant pulse dosage amount followed by repeated dosage amount of the
14 beneficial drugs 3 to 4 hours later. The dosage form provided by the
15 invention comprises within a single dosage form a first dose and a
16 repeat dose substantial equivalent to multiples of twice, thrice a day
17 or the like.

EXAMPLE 11

18
19 A dosage form comprising dimenhydrinate indicated for the
20 prevention and the treatment of nausea, vomiting or vertigo of motion
21 sickness is prepared according to the procedure of Example 10. The
22 dosage form comprises 50 mg of dimenhydrinate in the first layer and
23 50 mg of dimenhydrinate in the outer pulsed dose. The dosage form is
24 indicated for preventing motion sickness by taking the dosage form 1/2
25 to 1 hour before starting the activity, thereby providing a first
26 instant dose followed by a repeat dose 3 to 4 hours later from the
27 same dosage form.

28

1 EXAMPLE 12

2 A dosage form comprising two independently administrable
3 doses with the administration of a first dose followed by the adminis-
4 tration of a second dose at a later time from the same, single dosage
5 form is made according to the above procedures. In this example, the
6 dosage form comprises an internal 5 mg dose of methamphetamine hydro-
7 chloride, an anorectic for use in obesity, in the first layer, and 5 mg
8 of the same anorectic in the outermost first dose coat. The dosage
9 form can be administered once a day taken one-half hour before a meal,
10 usually before breakfast or lunch.

11 EXAMPLE 13

12 A dosage form for use as a nighttime cough relief up to 12
13 full hours is manufactured as described in Example 8. The dosage form
14 of this example comprises two doses in a single dosage form indicated
15 for convenient b.i.d. dosing that helps quiet coughs during the night.
16 The exterior first dose of the dosage form comprises 15 mg of dextro-
17 methorphan HBr, and the later delivered second dose comprises 15 mg of
18 dextromethorphan HBr. The dosage form is administered orally on
19 retiring for substantially avoiding interrupted rest.

20 EXAMPLE 14

21 A single dosage form comprising two distinct and timed
22 separate doses useful for administering the antihistamine
23 chlorprophenpyridamine maleate is manufactured as described above.
24 The dosage form comprises an immediately timed released external first
25 dose comprising 6 mg of chlorprophenpyridamine and a later timed
26 released second dose comprising 6 mg of chlorprophenpyridamine for
27 producing approximately ten hours symptomatic antihistamine relief to
28 the recipient.

EXAMPLE 15

A dosage form for use as a sleep-aid is provided by following the above manufacture procedures. The dosage form of this example comprises an internal compartment 26, drug formulation 27 comprising 60 mg of diphenhydramine hydrochloride and 340 mg of polyethylene oxide having a molecular weight of 10,000. The drug formulation 27 is surrounded with a delay lamina comprising hydroxypropyl cellulose and then with a lamina comprising cellulose acetate having an acetyl content of 32%. An exterior lamina for providing an instant pulse dosage of 20 mg of diphenhydramine hydrochloride, hydroxypropyl cellulose and adipic acid. The dosage form comprises a first and a second passageway, and when in operation it provides an instant first dose followed by delayed second dose delivered 3 to 3 1/2 hours later.

EXAMPLE 16

The above procedures are followed in this example for manufacturing a dosage form comprising a first pulse of 0.15 mg of the sedative triazolam and a later time delayed second pulse of 0.1 mg of triazolam.

In summary, it will be readily appreciated that the present invention contributes to the art an unobvious dosage form manufactured as a drug delivery device possessing wide and practical application. While the invention has been described and pointed out in detail and with reference to operative embodiments thereof, it will be understood that those skilled in the art will appreciate that various changes, modifications, substitutions and omissions can be made without departing from the spirit of the invention. It is intended, therefore, that the invention embrace those equivalents within the scope of the claims which follow.

THE EMBODIMENTS OF THE INVENTION IN WHICH AN EXCLUSIVE PROPERTY OR PRIVILEGE IS CLAIMED ARE DEFINED AS FOLLOWS:

1. A dosage form for the delivery of a beneficial drug formulation to an environment of use, comprising:

(a) a wall comprising in at least a part a semipermeable composition permeable to the passage of an external fluid present in the environment of use and substantially impermeable to the passage of a beneficial drug formulation, which wall surrounds and defines:

(b) a compartment;

(c) a first layer comprising a beneficial drug formulation in the compartment;

(d) a second layer comprising a hydrogel composition that increases in volume in the presence of fluid that enters the compartment;

(e) means for delaying the delivery of drug formulation from the compartment, which means comprises a drug-free composition that surrounds the first and second layer; and,

(f) at least one exit means in the wall for communicating the exterior of the dosage form with the compartment for delivering the drug formulation from the dosage form.

2. The dosage form for the delivery of the beneficial drug formulation to an environment of use according to claim 1, wherein the exit means is a passageway in the wall.

C

3. The dosage form for the delivery of the beneficial drug formulation to an environment of use according to claim 1, wherein the exit means is formed by fluid removing an exit forming composition from the wall.

4. The dosage form for the delivery of the beneficial drug formulation to an environment of use according to claim 1, wherein the first layer comprises the drug formulation and a hydrogel composition.

5. The dosage form for the delivery of the beneficial drug formulation to an environment of use according to claim 1, wherein the first layer comprises a hydrogel composition that is different than the hydrogel composition in the second layer.

6. The dosage form for delivery of the beneficial drug according to claim 1, wherein the dosage form comprises a first dose and a second dose administrable at a later time from the same dosage form.

7. A dosage form for delivering a beneficial drug formulation to an environment of use, wherein the dosage form comprises:

(a) a wall comprising in at least a part a semipermeable composition permeable to the passage of an external fluid present in the environment of use and substantially impermeable to the passage of a beneficial drug formulation, said wall surrounding:

1297368

26

67696-104

(1) a first layer comprising a dosage amount of a beneficial drug formulation;

(2) a second layer comprising a hydrogel composition that expands in the presence of fluid;

(3) means coated around the first and second layers for delaying the release of the drug formulation from the dosage form;

(b) at least one exit means in the wall for releasing the beneficial dosage formulation from the dosage form; and,

(c) a dosage amount of a beneficial drug formulation in contact with the exterior surface of the wall of the dosage form.

8. The dosage form for delivering the beneficial drug formulation to an environment of use according to claim 7, wherein the exit means in the wall is formed when the dosage form is in the environment of use.

9. The dosage form for delivering the beneficial drug formulation to an environment of use according to claim 7, wherein the exit means is a pore formed by leaching a pore former from the wall when the dosage form is in a fluid environment of use.

10. The dosage form for the delivery of the beneficial drug formulation to an environment of use according to claim 7, wherein the exit means and the first layer are present in the same area of the dosage form.

11. The dosage form for the delivery of the beneficial drug formulation to an environment of use according to claim 7, wherein the first layer comprises a hydrogel composition that is different than the hydrogel composition in the second layer.

12. A dosage form for the delivery of the beneficial agent midazolam to an environment of use, wherein the dosage form comprises:

(a) a wall comprising in at least a part a composition permeable to the passage of an external fluid present in the environment of use, which wall surrounds and defines:

(b) a compartment;

(c) a first layer comprising midazolam as a beneficial drug formulation in the compartment;

(d) a second layer comprising a hydrogel composition that exhibits a volume increase in the presence of fluid that enters the compartment;

(e) means for delaying the delivery of midazolam from the compartment, which means comprises a midazolam-free composition that surrounds the first and second layer; and,

(f) at least one passageway in the wall connecting the exterior of the dosage form with the compartment for delivering midazolam from the dosage form.

1297368

28

67696-104

13. A dosage form for delivering the beneficial drug midazolam to an environment of use, wherein the dosage form comprises:

(a) a wall comprising in at least a part a composition permeable to the passage of an external fluid, said wall surrounding:

(1) a first layer comprising a dosage amount of midazolam as a beneficial drug formulation;

(2) a second layer comprising a hydrogel composition that swells in the presence of fluid;

(3) means coated around the first and second layers for delaying the release of midazolam from the dosage form;

(b) at least one passageway in the wall for delivering midazolam from the dosage form; and,

(c) a dosage amount of midazolam in contact with the exterior surface of the wall of the dosage form.

14. A dosage form useful as a night-time sleep-aid for delivering a time delayed dose of diphenhydramine to a recipient, wherein the dosage form comprises:

(a) a wall comprising in at least a part a semipermeable composition permeable to the passage of an external fluid and substantially impermeable to the passage of a drug formulation, said wall surrounding:

(1) a first layer comprising a dose of diphenhydramine as a beneficial drug formulation;

(2) a second layer comprising a hydrogel formulation that expands in the presence of fluid;

1297368

29

67696-104

(3) means coated around the first and the second layer for delaying the release of diphenhydramine from the dosage form;

(b) at least one exit means in the wall for releasing diphenhydramine from the dosage form.

15. A dosage form useful as a night-time sleep-aid for delivering a first dose and a time delayed second dose of diphenhydramine to a recipient, wherein the dosage form is according to claim 14 additionally including a dosage amount of a first dose of diphenhydramine on the exterior wall surface of the dosage form.

16. A dosage form comprising a dose of a beneficial drug formulation useful as a sleep-aid for administering to a recipient, said dosage form comprising:

(a) a first wall comprising in at least a part a semipermeable composition permeable to the passage of external fluid, said wall surrounding:

(b) a second wall comprising means for delaying release of a doxylamine formulation from the interior of the dosage form, said second wall surrounding:

(c) a first layer comprising a dose of doxylamine as a beneficial drug formulation;

(d) a second layer comprising a hydrogel formulation that swells in the presence of fluid; and,

(e) at least one exit means in the wall for releasing doxylamine formulation from the interior of the dosage form.

D.

17. A single dosage form comprising two doses of a beneficial drug formulation useful as a sleep-aid for administering to a recipient wherein the dosage form is according to claim 16 additionally including a dosage amount of a first dose of doxylamine formulation coated on the exterior surface of the dosage form.

18. A dosage form useful for the relief of motion sickness, said dosage form comprising:

(a) a wall comprising in at least a part a semipermeable composition permeable to the passage of an external fluid and substantially impermeable to the passage of drug formulation, which wall surrounds:

(1) a first layer comprising a timed delayed dosage amount of dimenhydrinate as a beneficial drug formulation;

(2) a second layer comprising a hydrogel formulation that increases in volume in the presence of fluid;

(3) means for the timed delay of dimenhydrinate formulation from the interior of the dosage form interposed between the wall and the first layer;

(b) exit means in the wall for releasing the timed delayed dose of dimenhydrinate formulation from the dosage form.

19. A dosage form useful for the relief of motion sickness, wherein the dosage form is according to claim 18 additionally including a dosage amount of a first immediate dose of dimenhydrinate on the exterior wall of the dosage form.

1297368

31

67696-104

20. A dosage form for use as a cough relief for delivering a timed delayed dose of dextromethorphan to a recipient, wherein the dosage form comprises:

(a) a wall comprising in at least a part a semipermeable composition permeable to the passage of an external fluid and substantially impermeable to the passage of drug formulation, which wall surrounds:

(1) a dosage amount of dextromethorphan as a beneficial drug formulation;

(2) a hydrogel composition that increases in volume in the presence of fluid, said hydrogel composition in contact with the dextromethorphan formulation;

(3) means for delaying the release of the dextromethorphan formulation from the dosage form, said means interposed between the wall and the dextromethorphan formulation;

(b) at least one exit passageway in the wall for releasing the dextromethorphan formulation from the dosage form.

21. A dosage form for use as a cough relief for delivering an immediate dose and a timed delayed dose of dextromethorphan to a recipient, wherein the dosage form is according to claim 20 additionally including a dosage amount of an immediate dose of a dextromethorphan carried by the exterior surface of the wall of the dosage form.


SMART & BIGGAR
OTTAWA, CANADA

PATENT AGENTS

D

1237368

2-1

FIG.1

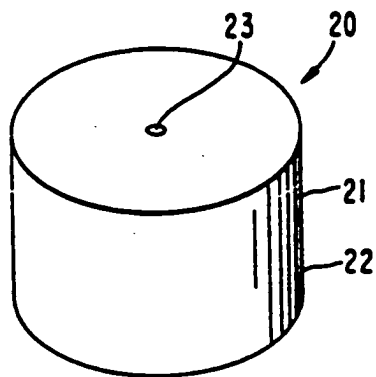


FIG.2

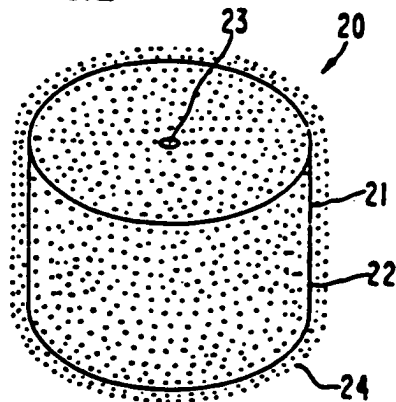
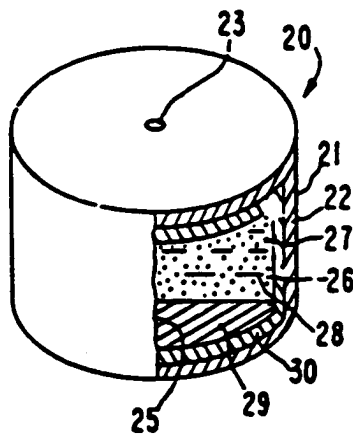


FIG.3



Patent Agents
Smart & Biggar

FIG. 4

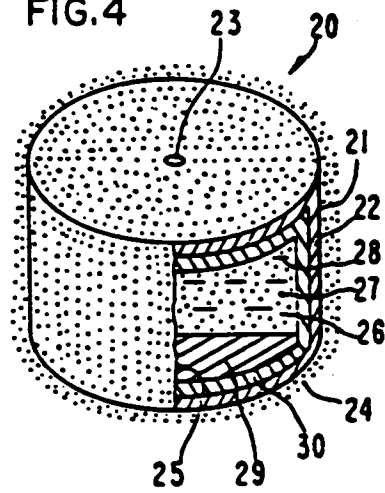


FIG. 5

